# Robust image recovery via total-variation minimization

Deanna Needell

Claremont McKenna College

Joint work with Rachel Ward Level Set Seminar, UCLA, July 2012

#### Collaborator

Joint work with Rachel Ward [ Univ. of Texas, Austin ]



D. Needell and R. Ward. Stable image reconstruction using total variation minimization, Submitted, Mar. 2012.

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## Outline

- Compressed Sensing (CS)
  - Applications
  - Mathematical Formulation & Methods
- Extensions to other dictionaries
  - Applications
  - Mathematical Formulation & Methods
- Imaging with CS
  - Theoretical possibilities
  - Total Variation
  - Empirical observations
  - New Results
  - Proof Sketch

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## The mathematical problem (notation)

## **③** Signal of interest $f \in \mathbb{C}^d (= \mathbb{C}^{N \times N})$

- **2** Measurement operator  $\mathcal{A} : \mathbb{C}^d \to \mathbb{C}^m$ .
- Measurements  $y = Af + \xi$ .



Problem: Reconstruct signal f from measurements y

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Background and Notation Other sparsity types

## Sparsity

Measurements  $y = Af + \xi$ .



Assume *f* is sparse:

- In the coordinate basis:  $\|f\|_0 \stackrel{\text{def}}{=} |\operatorname{supp}(f)| \leq s \ll d$
- In orthonormal basis: f = Bx where  $||x||_0 \le s \ll d$
- In other dictionary: f = Dx where  $||x||_0 \le s \ll d$

In practice, we encounter compressible signals.

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## **Digital Cameras**

#### Save your pennies to buy the new digital camera?



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## MRI

Feeling claustrophobic?

It'll only last a quick 45 minutes...



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## MRI



Figure 1: Example of a simple recovery problem. (a) The Logan-Shepp phantom test image. (b) Sampling domain  $\Omega$  in the frequency plane; Fourier coefficients are sampled along 22 approximately radial lines. (c) Minimum energy reconstruction obtained by setting unobserved Fourier coefficients to zero. (d) Reconstruction obtained by minimizing the total variation, as in (1.1). The reconstruction is an exact replica of the image in (a).

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### Pediatric MRI



(a-d) Submillimeter near-isotropic-resolution contrast-enhanced Ti-weighted MR images in 8-year-old boy. (a, c) Standard (b, d) compressed sensing reconstruction images. (c, d) Scomed images show improved delineation of the pancreatic duct (wretical arrow), zone (horizontal arrow), and galibladder wall (arrowhead), and equivalent definition of potial vein (black arrow) with L1 STPR-Ti reconstruction.

(Caffey Award : Faster Pediatric MRI Via Compressed Sensing - Shreyas Vasanawala et.al. (Stanford University))

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## Many more...

- Radar
- Error Correction
- Computational Biology (DNA Microarrays)
- Geophysical Data Analysis
- Data Mining, classification
- Neuroscience
- Imaging
- ...

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## Sparsity...

## Sparsity in coordinate basis: f=x



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## Reconstructing the signal f from measurements y

#### $\ell_1$ -minimization [Candès-Romberg-Tao]

Let A satisfy the Restricted Isometry Property and set:

$$\hat{f} = \underset{g}{\operatorname{argmin}} \|g\|_1 \quad \text{such that} \quad \|\mathcal{A}f - y\|_2 \leq \varepsilon,$$

where  $\|\xi\|_2 \leq \varepsilon$ . Then we can stably recover the signal f:

$$\|f-\hat{f}\|_2 \lesssim \varepsilon + \frac{\|x-x_s\|_1}{\sqrt{s}}.$$

This error bound is optimal.

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## Restricted Isometry Property

•  $\mathcal{A}$  satisfies the Restricted Isometry Property (RIP) when there is  $\delta < c$  such that

$$(1-\delta)\|f\|_2\leq \|\mathcal{A}f\|_2\leq (1+\delta)\|f\|_2$$
 whenever  $\|f\|_0\leq s.$ 

• Gaussian or Bernoulli measurement matrices satisfy the RIP with high probability when

$$m \gtrsim s \log d$$
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• Random Fourier and others with fast multiply have similar property:  $m \gtrsim s \log^4 d$ .

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## Sparsity...



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## Natural Images

Images are compressible in Wavelet bases.







Figure: Haar basis functions

Wavelet transform is orthonormal and multi-scale. Sparsity level of image is higher on detail coefficients.

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Figure: Boats image, 2D Haar transform, and compression from 10% of Haar coefficients

$$X = H^{-1}H(X) = \sum_{j,k=1}^{N} c_{j,k}H_{j,k}$$

X is s-sparse (in Haar basis) if  $\|c\|_0 \leq s$ 

X<sup>w</sup><sub>s</sub> is the best *s*-term approximation to X in Haar basis

Image compression:  $X \to X_s^w$ 

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## Sparsity in orthonormal basis B

#### L1-minimization Method

For orthonormal basis B, f = Bx with x sparse, one may solve the  $\ell_1$ -minimization program:

$$\hat{f} = \operatorname*{argmin}_{ ilde{f} \in \mathbb{C}^n} \|B^{-1} \tilde{f}\|_1$$
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Same results hold.

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## Sparsity...

## In arbitrary dictionary: f = Dx



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## The CS Process



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## Example: Oversampled DFT

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• 
$$n \times n$$
 DFT:  $d_k(t) = \frac{1}{\sqrt{n}}e^{-2\pi i k t/n}$ 

- $\bullet$  Sparse in the DFT  $\to$  superpositions of sinusoids with frequencies in the lattice.
- Instead, use the oversampled DFT:
- Then D is an overcomplete frame with highly coherent columns → conventional CS does not apply.
Background and Notation Other sparsity types

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#### Example: Gabor frames



## • Gabor frame: $G_k(t) = g(t - k_2 a)e^{2\pi i k_1 b t}$

- Radar, sonar, and imaging system applications use Gabor frames and wish to recover signals in this basis.
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## Example: Curvelet frames



# • A Curvelet frame has some properties of an ONB but is overcomplete.

- Curvelets approximate well the curved singularities in images and are thus used widely in image processing.
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# Example: UWT



- The undecimated wavelet transform has a translation invariance property that is missing in the DWT.
- The UWT is overcomplete and this redundancy has been found to be helpful in image processing.
- Again, this means D is a redundant dictionary → conventional CS does not apply.

Background and Notation Other sparsity types

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#### $\ell_1$ -Synthesis Method

For arbitrary tight frame D, one may solve the  $\ell_1$ -synthesis program:

$$\hat{f} = D\left( \operatorname*{argmin}_{\tilde{x} \in \mathbb{C}^n} \| \tilde{x} \|_1 \text{ subject to } \| \mathcal{A}D\tilde{x} - y \|_2 \leq \varepsilon 
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Some work on this method [Candès et.al., Rauhut et.al., Elad et.al.,...]

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#### $\ell_1$ -Analysis Method

For arbitrary tight frame D, one may solve the  $\ell_1$ -analysis program:

$$\hat{f} = \operatorname*{argmin}_{ ilde{f} \in \mathbb{C}^n} \|D^* \tilde{f}\|_1$$
 subject to  $\|\mathcal{A} \tilde{f} - y\|_2 \leq \varepsilon_1$ 

# Condition on A?

#### D-RIP

We say that the measurement matrix A obeys the *restricted* isometry property adapted to D (D-RIP) if there is  $\delta < c$  such that

 $(1-\delta)\|Dx\|_2^2 \le \|\mathcal{A}Dx\|_2^2 \le (1+\delta)\|Dx\|_2^2$ 

holds for all *s*-sparse *x*.

Similarly to the RIP, many classes of random matrices satisfy the D-RIP with  $m \approx s \log(d/s)$ . Randomly perturbed RIP matrices satisfy D-RIP [Krahmer-Ward '11], or similar property, Weibull matrices [Foucart '12], ...

Background and Notation Other sparsity types

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## CS with tight frame dictionaries

#### Theorem [Candès-Eldar-N-Randall]

Let *D* be an arbitrary tight frame and let  $\mathcal{A}$  be a measurement matrix satisfying D-RIP. Then the solution  $\hat{f}$  to  $\ell_1$ -analysis satisfies

$$\|\hat{f} - f\|_2 \lesssim \varepsilon + \frac{\|D^*f - (D^*f)_s\|_1}{\sqrt{s}}$$

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Background and Notation Other sparsity types

## Implications

#### In other words,

This result says that  $\ell_1$ -analysis is very accurate when  $D^*f$  has rapidly decaying coefficients and D is a tight frame. This is the case in for example applications using the Oversampled DFT, Gabor frames, Undecimated WT, and Curvelet frames.

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## **Experimental Setup**

n = 8192, m = 400, d = 491, 520A:  $m \times n$  Gaussian, D:  $n \times d$  Gabor



Figure: The signal is a superposition of 6 radar pulses, each of which being about 200 ns long, and with frequency carriers distributed between 50 MHz and 2.5 GHz (top plot). As can be seen, three of these pulses overlap in the time domain.

Defining Sparsity

New Results

Background and Notation Other sparsity types

## **Experimental Results**



Figure: Portion of the matrix  $D^*D$ , in log-scale (left). Sorted analysis coefficients (in absolute value) of the signal from Figure 3 (right).

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## **Experimental Results**



Figure: Recovery in both the time (below) and frequency (above) domains by  $\ell_1$ -analysis. Blue denotes the recovered signal, green the actual signal, and red the difference between the two.

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Other sparsifying transforms for images?

Background and Notation Other sparsity types

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Other sparsifying transforms for images?

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Imaging with CS Imaging: Mathematical Formulation

# Natural images

Sparse...



 $256\times256$  "Boats" image

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Imaging with CS Imaging: Mathematical Formulation

# Natural images

Sparse wavelet representation...





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Imaging with CS Imaging: Mathematical Formulation

# Natural images

Images are compressible in *discrete gradient*.





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Imaging with CS Imaging: Mathematical Formulation

# Natural images

#### Images are compressible in *discrete gradient*.



The discrete directional derivatives of an image  $f\in \mathbb{C}^{N imes N}$  are

$$\begin{aligned} f_x : \mathbb{C}^{N \times N} &\to \mathbb{C}^{(N-1) \times N}, \qquad (f_x)_{j,k} = f_{j,k} - f_{j-1,k}, \\ f_y : \mathbb{C}^{N \times N} &\to \mathbb{C}^{N \times (N-1)}, \qquad (f_y)_{j,k} = f_{j,k} - f_{j,k-1}, \end{aligned}$$

the discrete gradient operator is

$$\nabla[f] = (f_x, f_y)$$

Imaging with CS Imaging: Mathematical Formulation

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Imaging with CS Imaging: Mathematical Formulation

# Natural Notation

Images are compressible in discrete gradient.



- $||f||_p := \left(\sum_{j=1}^N \sum_{k=1}^N |f_{j,k}|^p\right)^{1/p}$
- *f* is *s*-sparse if  $||f||_0 := \{\#(j,k) : f_{j,k} \neq 0\} \le s$
- $f_s$  is the best *s*-sparse approximation to f
- "Phantom":  $\|\nabla[f]\|_0 = .03N^2$
- "Boats":  $\|\nabla[f] \nabla[f]_s\|_2$  decays quickly in s

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Imaging with CS Imaging: Mathematical Formulation

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Imaging with CS Imaging: Mathematical Formulation

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Imaging with CS Imaging: Mathematical Formulation

# Natural Notation

Images are compressible in discrete gradient.



• 
$$||f||_p := \left(\sum_{j=1}^N \sum_{k=1}^N |f_{j,k}|^p\right)^{1/p}$$

- f is s-sparse if  $\|f\|_0 := \{\#(j,k) : f_{j,k} \neq 0\} \le s$
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Imaging with CS Imaging: Mathematical Formulation

## Sparsity in gradient

### CS Theory

The gradient operator  $\boldsymbol{\nabla}$  is not an orthonormal basis or a tight frame.

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Imaging with CS Imaging: Mathematical Formulation

Comparison of two compressed sensing reconstruction algorithms

### Haar-minimization $(L_1$ -Haar)

 $\hat{f}_{Haar} = \operatorname{argmin} \|H(Z)\|_1$  subject to  $\|\mathcal{A}Z - y\|_2 \leq \varepsilon$ 

#### Total Variation minimization (TV)

 $\hat{f}_{TV} = \operatorname{argmin} \|\nabla[Z]\|_1$  subject to  $\|\mathcal{A}Z - y\|_2 \leq \varepsilon$ , where  $\|Z\|_{TV} = \|\nabla[Z]\|_1$  is the *total-variation norm*.

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Imaging with CS Imaging: Mathematical Formulation

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Imaging with CS Imaging: Mathematical Formulation

# Imaging via compressed sensing



(a) Original



(b) TV (c) *L*<sub>1</sub>-Haar

Figure: Reconstruction using  $m = .2N^2$ 

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Imaging with CS Imaging: Mathematical Formulation

# Imaging via compressed sensing



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Figure: Reconstruction using  $m = .2N^2$  measurements

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Imaging with CS Imaging: Mathematical Formulation

# Imaging via compressed sensing



(a) Original



Figure: Reconstruction using  $m = .2N^2$  measurements.

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Imaging with CS Imaging: Mathematical Formulation

# Imaging via compressed sensing



(a) (Quantization)



(b) TV (c) *L*<sub>1</sub>-Haar

Figure: Reconstruction using  $m = .2N^2$  measurements

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Imaging with CS Imaging: Mathematical Formulation

# Imaging via compressed sensing



(a) (Gaussian)



(b) TV Deanna Needell

Imaging with CS Imaging: Mathematical Formulation

## Imaging via compressed sensing

## InView (Austin TX)



Figure: SWIR Reconstruction using  $m = .5N^2$  measurements

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Imaging with CS Imaging: Mathematical Formulation

## Imaging via compressed sensing

InView (Austin TX)



#### Figure: InView SWIR camera

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Imaging with CS Imaging: Mathematical Formulation

# Empirical $\rightarrow$ Theoretical?

#### TV Works

Empirically, it has been well known that

$$\hat{f}_{TV} = \operatorname{argmin} \|Z\|_{TV} \text{ subject to } \|\mathcal{A}Z - y\|_2 \le \varepsilon, \quad (TV)$$

provides quality, stable image recovery.

No provable stability guarantees.

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Movies, higher dimensional objects?

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Robust image recovery via total-variation minimization

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First results on stability of TV

## **Proof Sketch**

## Strengthened Sobolev inequalities for random subspaces

Deanna Needell Robust image recovery via total-variation minimization

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# **Discrete Sobolev inequalities**

Proposition (Sobolev inequality for discrete images)

Let  $X \in \mathbb{R}^{N \times N}$  be mean-zero. Then

 $||X||_2 \le ||X||_{TV}$ 

Proposition (New: Strengthed Sobolev inequality)

With probability  $\geq 1 - e^{-cm}$ , the following holds for all images  $X \in \mathbb{R}^{N \times N}$  in the null space of an  $m \times N^2$  random Gaussian matrix

$$\|X\|_{2} \lesssim \frac{[\log(N)]^{3/2}}{\sqrt{m}} \|X\|_{TV}$$

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Proof ingredients:

• [CDPX 99:] Denote the bivariate Haar wavelet coefficients of  $X \in \mathbb{R}^{N \times N}$  by  $c_{(1)} \ge c_{(2)} \ge \cdots \ge c_{(N^2)}$ . Then

$$|c_{(k)}| \lesssim \frac{\|X\|_{TV}}{k}$$

That is, the sequence is in weak- $\ell_1$ .

If Φ : ℝ<sup>d</sup> → ℝ<sup>m</sup> has (properly normalized) i.i.d. Gaussian entries then with probability exceeding 1 − e<sup>-cm</sup>, Φ has the RIP of order s ~  $\frac{m}{\log d}$ :

$$\frac{3}{4} \|f\|_2 \le \|\Phi f\|_2 \le \frac{5}{4} \|f\|_2$$
 for all *s*-sparse *f*.

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Let  $\Phi : \mathbb{R}^d \to \mathbb{R}^m$  be a Gaussian matrix and  $\Phi X = 0$ .

Suppose that  $\Psi = \Phi \mathcal{H}^* : \mathbb{R}^d \to \mathbb{R}^m$  has the RIP of order 2*s*.

Decompose  $c = \mathcal{H}X$  into *s*-sparse blocks  $c = c_{S_0} + c_{S_1} + c_{S_2} + \dots$ 

$$\begin{split} 0 &\geq \|\Psi(c_{S_0} + c_{S_1})\|_2 - \sum_{j \geq 2} \|\Psi c_{S_j}\|_2 \\ (\mathsf{RIP of } \Psi) &\geq \frac{3}{4} \|c_{S_0} + c_{S_1}\|_2 - \frac{5}{4} \sum_{j \geq 2} \|c_{S_j}\|_2 \end{split}$$

$$(\text{block trick}) \geq \frac{3}{4} \|c_{S_0}\|_2 - \frac{5/4}{\sqrt{s}} \sum_{j \geq 1} \|c_{S_j}\|_1$$

$$(c \text{ in weak } \ell_1) \ge \frac{3}{4} \|c_{S_0}\|_2 - \frac{5/4}{\sqrt{s}} \|X\|_{TV} \log(d/s)$$

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(c in weak  $\ell_1$ )  $\ge \frac{3}{4} \|c_{S_0}\|_2 - \frac{5/4}{\sqrt{s}} \|X\|_{TV} \log(d/s)$ 

### So

$$\|c_{S_0}\|_2 \leq \frac{1}{\sqrt{s}} \|X\|_{TV} \log(d/s), \\ \|c - c_{S_0}\|_2 \leq \frac{1}{\sqrt{s}} \|X\|_{TV} \ (c \text{ is in weak } \ell_1)$$

### Then

$$\begin{split} \|X\|_2 &= \|c\|_2 \leq \|c_{S_0}\|_2 + \|c - c_{S_0}\|_2 \\ &\leq \frac{\log(d/s)}{\sqrt{s}} \|X\|_{TV} \end{split}$$

Proof is complete, because with probability  $1 - \varepsilon^{-cm}$ , RIP of  $\Phi \mathcal{H}^*$  holds with  $s \sim m/\log(d)$ .

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Stable signal recovery using total-variation minimization

## Method of proof:

- First prove stable *gradient* recovery
- Translate stable gradient recovery to stable signal recovery using the strengthened Sobolev inequality.

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#### Remove the log factor?

- Our results do not immediately hold for vectors. What about stable (1D) signal recovery?
- Patel, Maleh, Gilbert, Chellappa '11] Images are even sparser in individual directional derivatives f<sub>x</sub>, f<sub>y</sub>. If we minimize separately over directional derivatives, can we still prove stable recovery?
- Other optimization problems

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First results on stability of TV

### Movies are very sparse!



- Movies are very sparse in all three dimensions
- Silicon Retina (Institute of Neuroinformatics) is the design of a camera that mimics retinas
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First results on stability of TV

# Fast vision in bad lighting

#### Figure: ("RoboGoalie", Silicon Retina, Institute of Neuroinformatics)

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First results on stability of TV

# Fluid Particle Tracking Velocimetry

#### Figure: ("PTV", Silicon Retina, Institute of Neuroinformatics)

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First results on stability of TV

## **Mobile Robotics**

Figure: ("Robotic Driver", Silicon Retina, Institute of Neuroinformatics)

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First results on stability of TV

### Sleep disorder research

Figure: ("Sleeping Mouse", Silicon Retina, Institute of Neuroinformatics)

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# Thank you!

### E-mail:

dneedell@cmc.edu

### Web:

• www.cmc.edu/pages/faculty/DNeedell

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